

**CE20:** Quantitative PET for Liver Diseases

12 June 2022 | Vancouver, Canada

## Dynamic Liver PET: Kinetic Modeling and Clinical Translation for NASH Imaging

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This work is supported by NIH R01 DK124803

## Disclosure

• University of California Davis has a revenue sharing agreement and a research agreement with United Imaging Healthcare (UIH)

## Nonalcoholic Steatohepatitis (NASH)



http://www.sydneynwgastro.com.au/

• 5-10% of nonalcoholic fatty liver disease patients develop NASH

 Diagnostic hallmark of NASH is liver inflammation in the setting of steatosis

## Gap in Clinical Imaging of NASH

<b>Disease Characteristics</b>	Clinical Imaging
Liver Steatosis	Magnetic Resonance Proton Density Fat Fraction (MR-PDFF) or Computed Tomography (CT)
Liver Inflammation	?
Liver Fibrosis	Magnetic Resonance Elastography (MRE), Ultrasound Elastography

#### Development and Translation of PET Methods for NASH Imaging

• A team of MDs and PhDs at UC Davis Medical Center



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## Standard <sup>18</sup>F-FDG PET for Evaluating Liver Inflammation?

Liver is the primary organ to store and regulate glucose

• <sup>18</sup>F-FDG PET is mainly used for assessing glucose metabolism

• Standard FDG PET measure did not correlate with liver inflammation



# Dynamic <sup>18</sup>F-FDG PET Imaging

 Dynamic PET monitors both spatial and temporal change of tracer uptake, creating a functional "movie"



Aorta

## Kinetic Quantification by Time Activity Curve (TAC) Fitting



• For FDG, conventional focus is on glucose metabolism

Net influx rate 
$$K_i = \frac{K_1 k_3}{k_2 + k_3}$$

• We call attention to glucose transport rates (e.g., K<sub>1</sub>) as well

# A Glucose Transport Hypothesis for Liver Inflammation

- Glucose is transported by glucose transporters (GLUTs)
- Chronic liver inflammation involves programmed cell deaths and may associate with low GLUTs expression



• Our hypothesis:

liver inflammation is associated with decreased glucose transport rate (measured by FDG  $K_1$ )

## Challenge with Kinetic Quantification in the Liver

- Liver has two blood supplies: hepatic artery and portal vein
- Dual-blood input function is required for accurate kinetic modeling



# Dual-blood Input Function (DBIF)

- Flow-weighted DBIF model  $C_p(t) = f_A C_A(t) + f_{PV} C_{PV}(t)$
- Typical weights measured with blood sampling in foxhounds
  - $-f_A$ : 20%
  - $-f_{PV}$ : 80%
- However, portal vein input can not be measured accurately from PET images



## Population-based DBIF: The Mathematical Model



Image taken from Feng et al TRPMS 2020

• Describe  $C_{PV}(t)$  as a convolutional model of  $C_A(t)$ 

$$C_{PV}(t) = C_A(t) \otimes h(t;\theta)$$

 h(t) is a dispersion function, accounting for the effect of tracer passing through the gastrointestinal tract, e.g.,

$$h(t) = k_a e^{-k_a t}$$

### Population-based DBIF: Determination from Animal Data

- More examples of the dispersion model h(t):
  - Brix et al 2001:  $h(t) = t^{P_0} (P_1 e^{-P_2 t} + P_3 e^{-P_4 t})$

– Winterdahl *et al* 2010:

$$h(t) = \beta/(t+\beta)^2$$

 Model parameters are determined from *animal* studies with blood sampling and then applied to *human* studies

### **Optimization-derived DBIF: General Concept**



- No blood sampling is required
- Directly applicable to human data

Chen et al TNS 2008; Kudomi et al EJNMMI 2009; Feng et al TRPMS 2020;

#### **Optimization-derived DBIF: Model for FDG**



**Differential Equations:** 

$$\frac{\mathrm{d}}{\mathrm{d}t} \begin{bmatrix} C_f(t) \\ C_m(t) \\ C_{PV}(t) \end{bmatrix} = \begin{bmatrix} -(k_2 + k_3) & k_4 & K_1(1 - f_A) \\ k_3 & -k_4 & 0 \\ 0 & 0 & -k_a \end{bmatrix} \begin{bmatrix} C_f(t) \\ C_m(t) \\ C_{PV}(t) \end{bmatrix} + \begin{bmatrix} K_1 f_A \\ 0 \\ k_a \end{bmatrix} C_A(t)$$

 All model parameters are structurally identifiable, though subject to local solutions

 Estimates of K<sub>1</sub> and influx rate K<sub>i</sub> are stable (low bias and variance)

### Impact of Liver DBIF on Parametric Imaging

#### Parametric images of FDG $K_1$



mL/min/mL

#### (a) w/o DBIF

(b) with DBIF

## Demonstration of Liver Inflammation and FDG K<sub>1</sub>



#### Liver Inflammation Was Associated with Decreased Glucose Transport

Liver glucose transport (K<sub>1</sub>)

Glucose metabolism (K<sub>i</sub>)



Sarkar et al. AJR 2019; CGH 2021

#### Can the Scan Duration Be Shortened?

 A 15-minute scan has a <5% difference in liver FDG-K<sub>1</sub> compared to the 60min reference



#### Feasibility of a 15-minute Scan Protocol





# What is FDG K<sub>1</sub> in the Liver?

• FDG K<sub>1</sub> represents the overall delivery rate of FDG from blood to liver tissue cells

- It is a mix of
  - Blood flow
  - Glucose-specific transport (from blood to the interstitial space and then to the intracellular space)



# Opportunities Open Up by High-performance Scanners

• Recent sensitivity **boost** on commercial PET scanners

4-40x

- High-temporal resolution (HTR, e.g., 1-2s/frame) may become feasible for dynamic PET imaging
- HTR potentially enables separation of the transport processes to measure

*blood flow* and *tracer-specific transport* rates

from a single-tracer dynamic scan

UIH uEXPLORER



194 cm

Siemens Quadra



### Acknowledgments

#### NIH funding: R01 DK124803

Dr. Siqi Li Dr. Ben Spencer Dr. Quyen Tran Dr. Yang Zuo

Alex Kuo Elizabeth Li Peter Liu Sean Romeo Yiran Wang Dr. Ramsey D. Badawi Dr. Shuai Chen Dr. Simon R. Cherry Dr. Jinyi Qi

Dr. Michael Corwin Dr. Victoria Lyo Dr. Karen Matsukuma Dr. Valentina Medici Dr. Kristin Olson Dr. Souvik Sarkar Denise Claude Heather Hunt Mike Nguyen Michael Rusnak